

CLEARANCE AND FICK'S PRINCIPLE

Stig P. Cramer, MD, PhD

Post Doc, Functional Imaging Unit

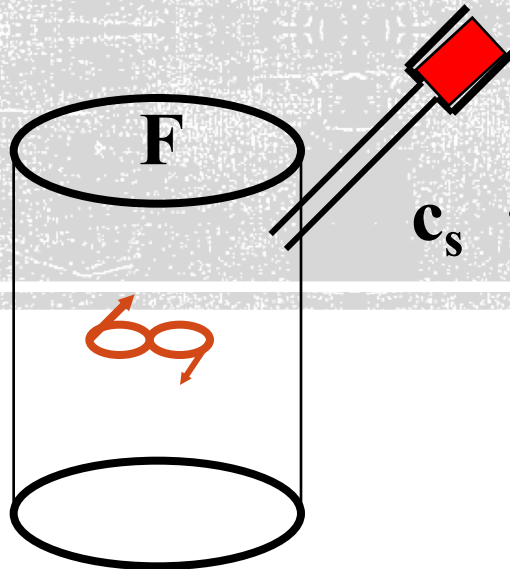
Rigshospitalet, Glostrup



INDICATOR-DILUTION METHODS

Constant Infusion (Stewart principle)

The aim : to measure the flow of an organ or a vessel or a pipeline



$$[F] = \text{ml/s}$$

$$c_s \cdot F_s = j_{in} \quad \text{flux !!!!}$$

$$[c_s] = \text{mmol/ml}$$

$$[F_s] = \text{ml/s}$$

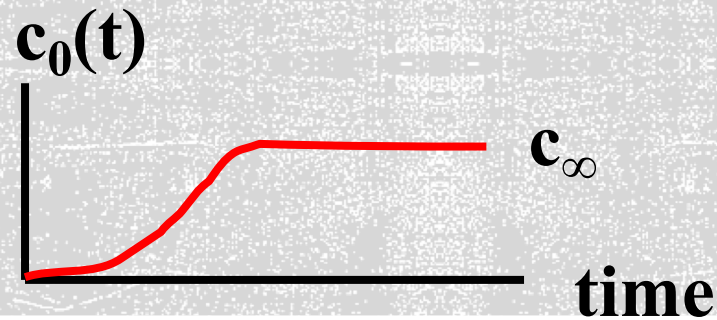
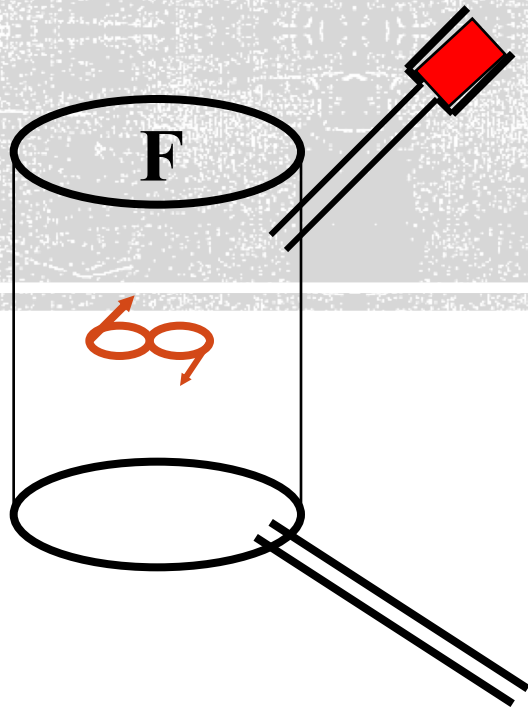
$$[j_{in}] = \text{mmol/s}$$



INDICATOR-DILUTION METHODS

Constant Infusion (Stewart principle)

The aim : to measure the flow of an organ or a vessel or a pipeline



$$j_{in} = j_o$$

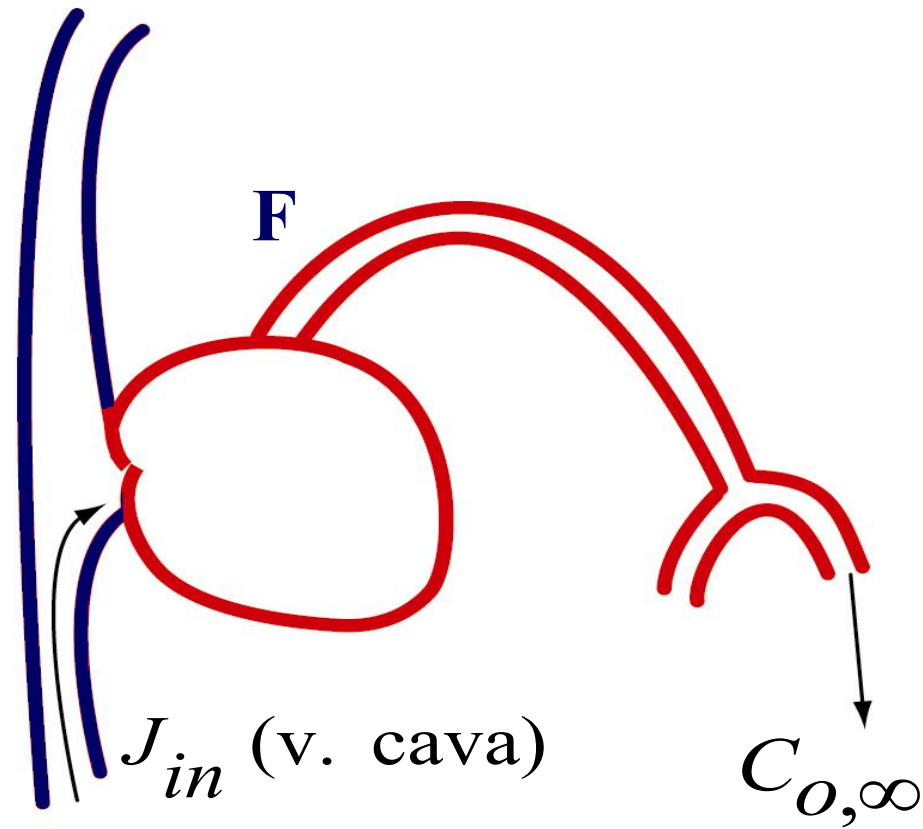
$$c_s \cdot F_s = (F + F_s) \cdot c_\infty$$

$$F = j_{in} / c_\infty$$



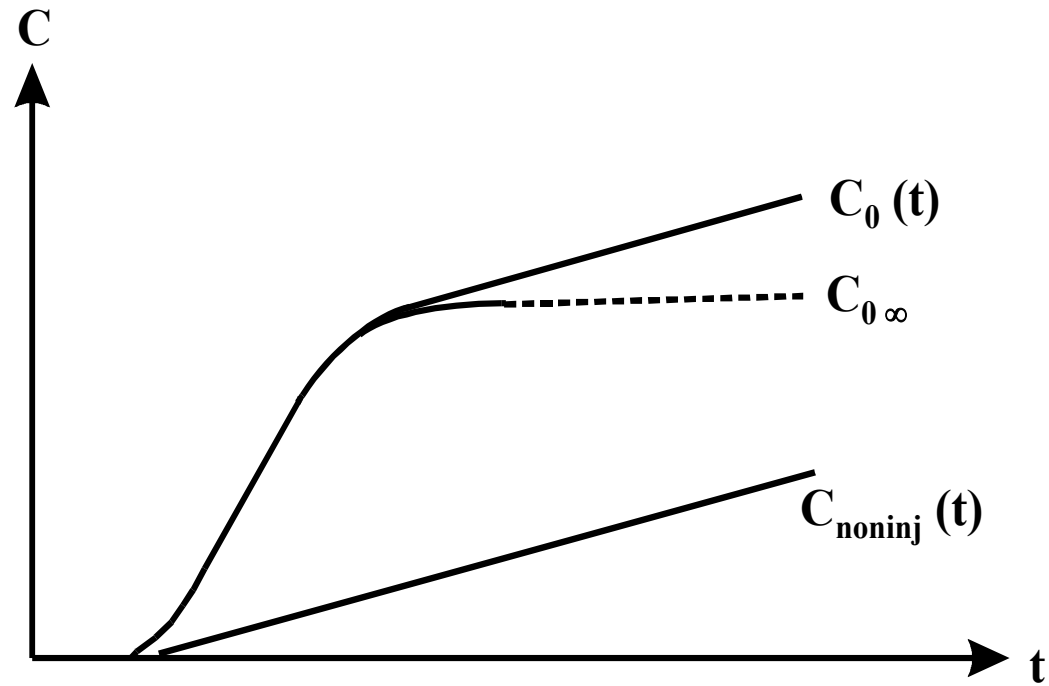
$$F \gg F_s$$

$c_0(t)$



Stewart's principle: Continuously infusion in vena cava, and outlet concentration measurement from a peripheral artery.





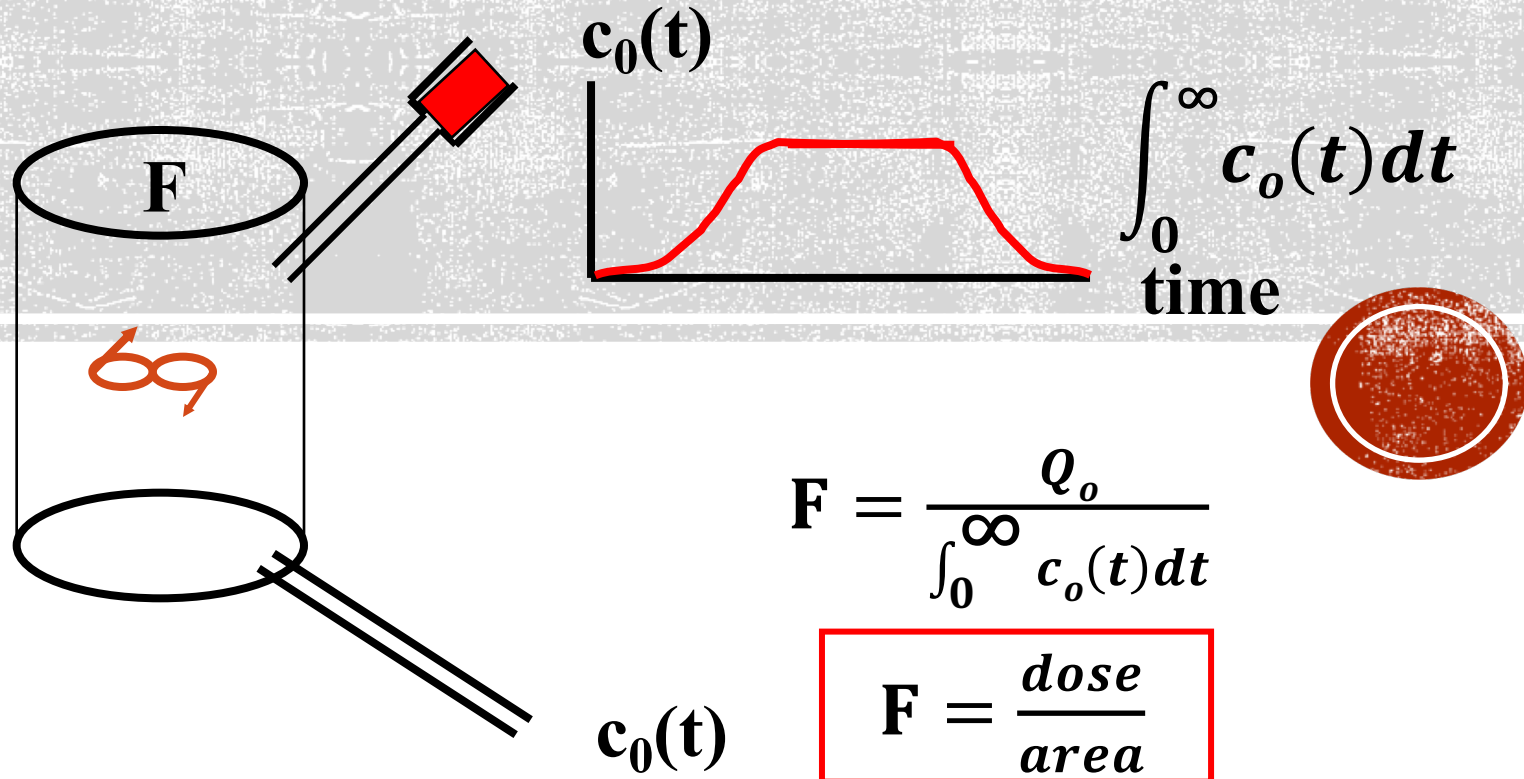
Measurement of concentration at the outlet and the "noninj" side.



BOLUS INJECTION

(Henriques and Hamilton)

The aim : to measure the flow of an organ or a vessel or a pipeline



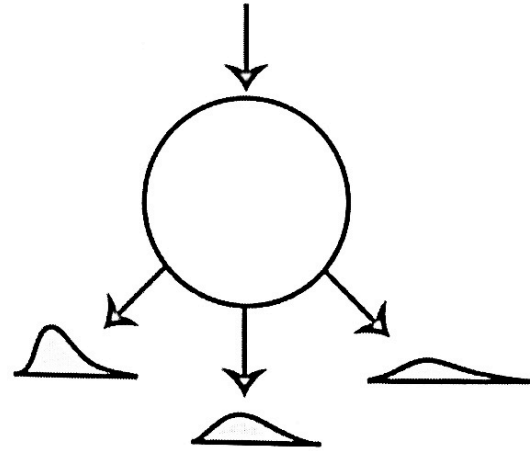
$$F = \frac{Q_o}{\int_0^{\infty} c_o(t) dt}$$

$$F = \frac{dose}{area}$$

RULE OF EQUIVALENT AREAS

(Sapirstein)

Reglen om ækvivalente arealer:



$$F = \frac{\text{dose}}{\text{area}}$$

Area is the same no matter where we sample
the C_0 curve!

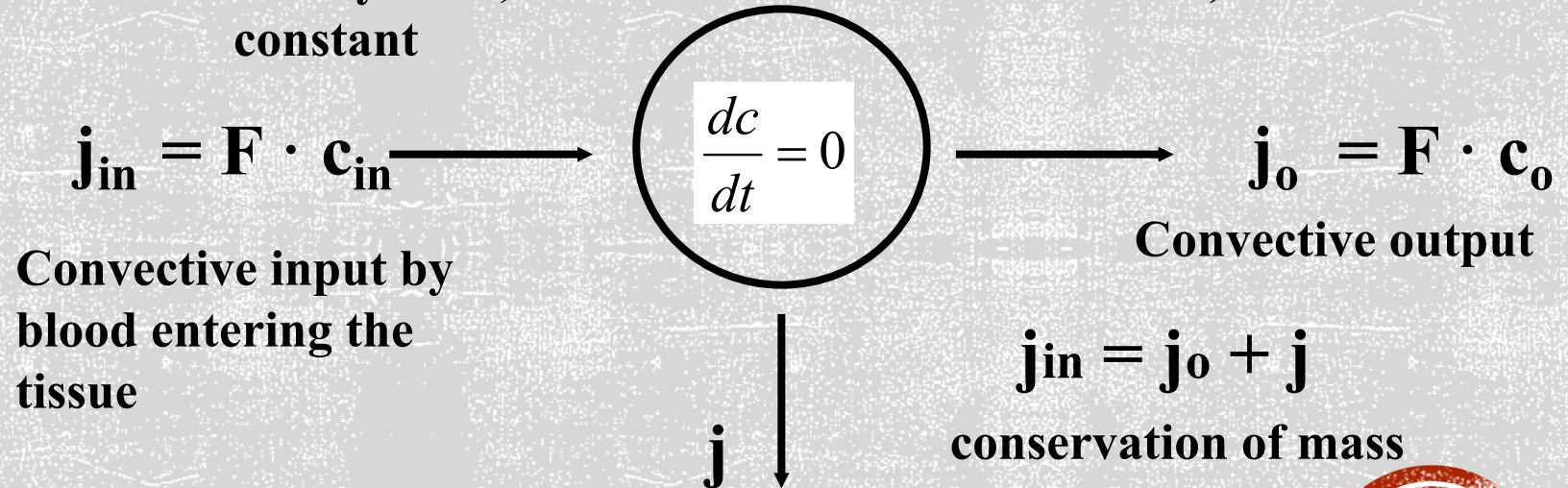
Fick's principle

The conservation of matter



FICK'S PRINCIPLE

Steady state; Concentration here is constant, fluxes are here constant



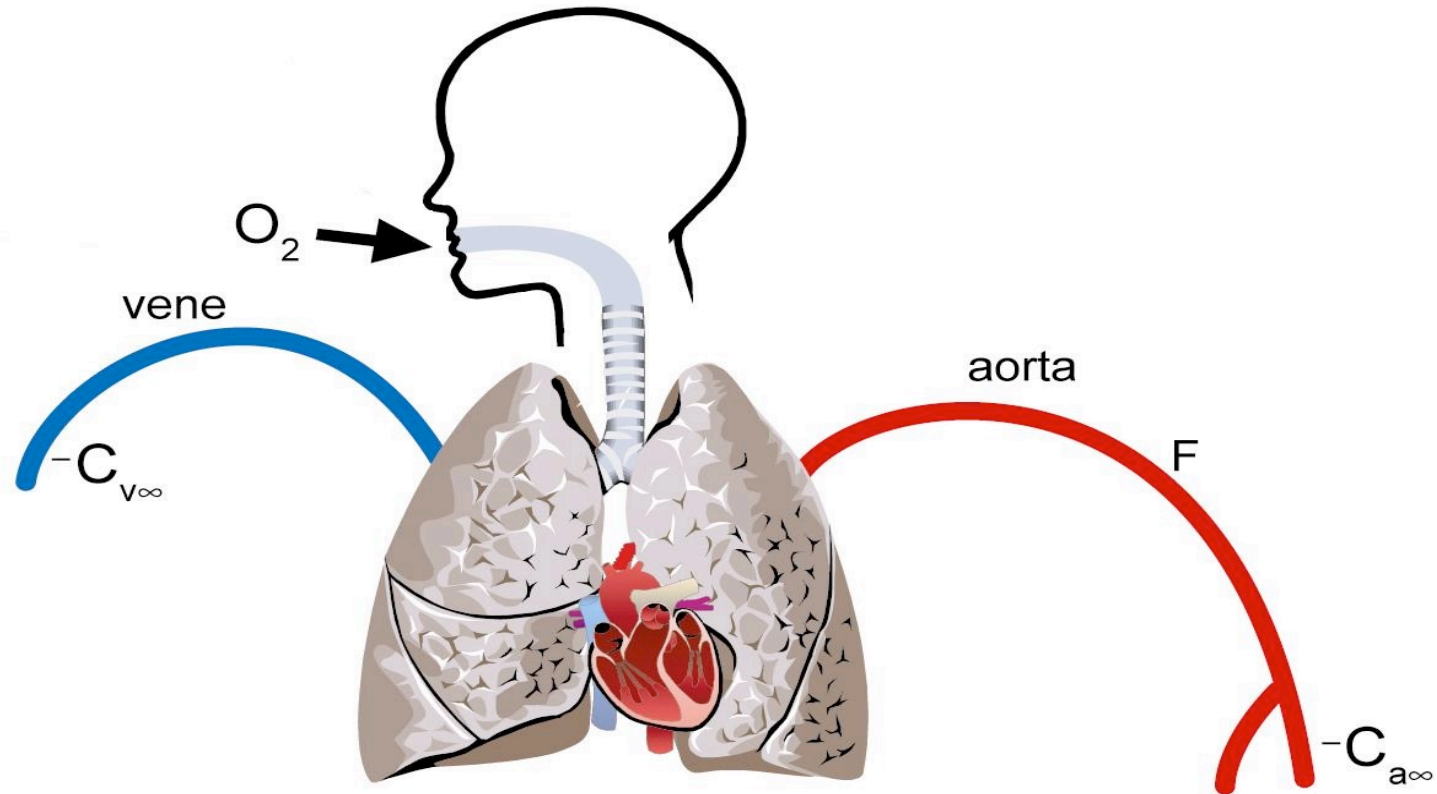
Non-convective uptake of a tissue

$$F \cdot c_{in} = F \cdot c_o + j$$

$$F = j / (c_{in} - c_o)$$



Fick's principle: cardiac output



$$J_a = J_{O_2} + J_v$$

$$F \cdot C_{a\infty} = J_{O_2} + F \cdot C_{v\infty} \Rightarrow$$

$$F = \frac{J_{O_2}}{C_{a\infty} - C_{v\infty}}$$



CEREBRAL METABOLIC RATE OF OXYGEN $CMRO_2$

- Fick's principle

blood sample

$$CMRO_2 = 4 \cdot [Hgb] \cdot CBF \cdot (S_a O_2 - S_v O_2)$$

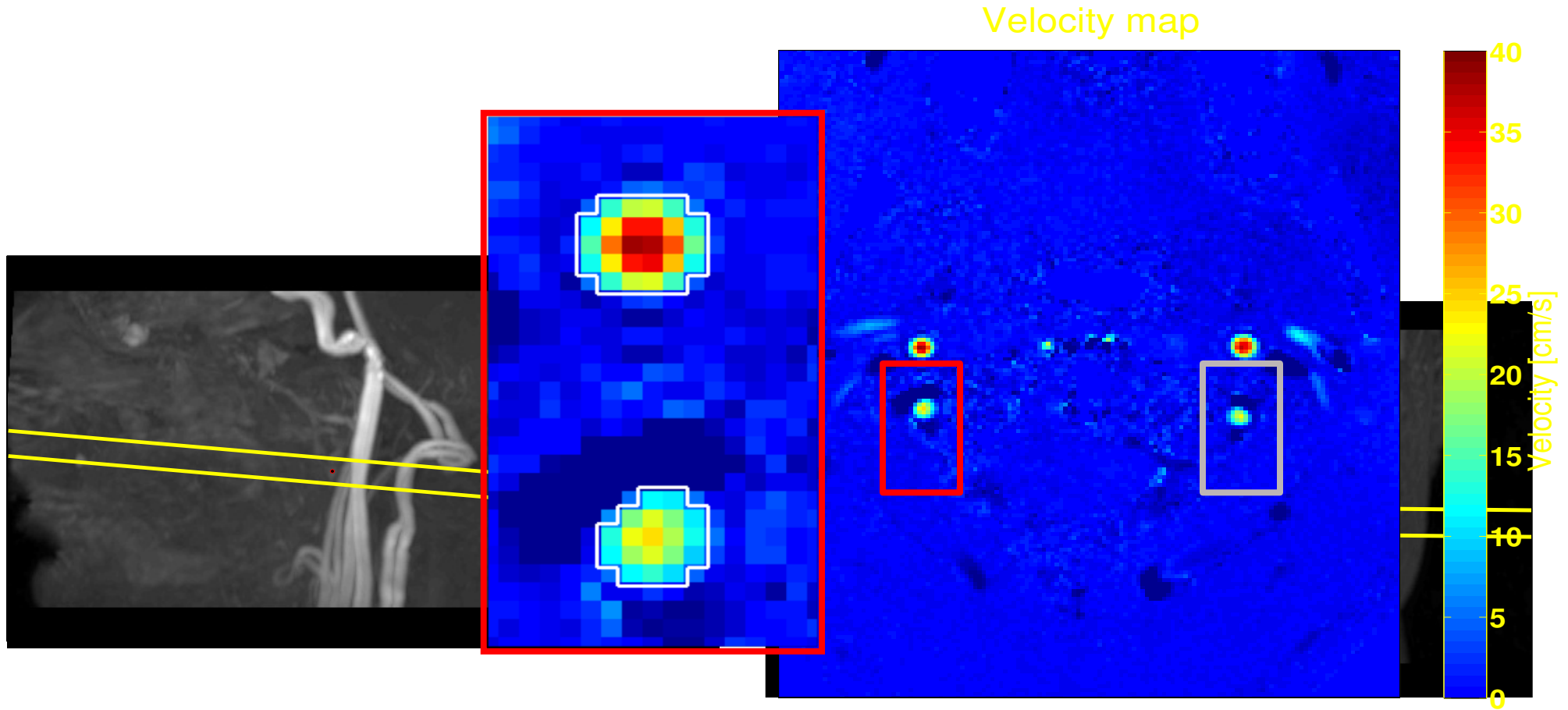
**MRI phase contrast
mapping**

**Puls-oximetri
(A-cath)**

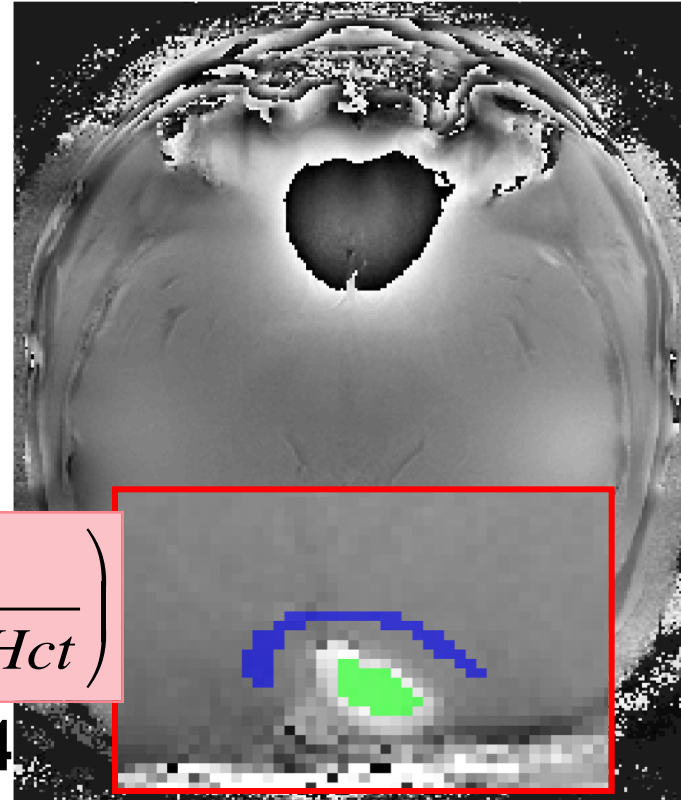
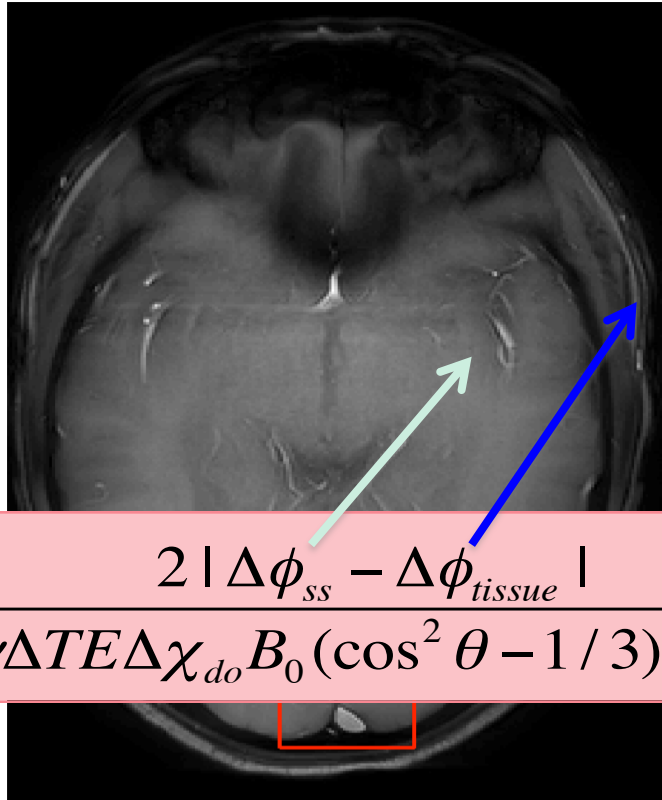
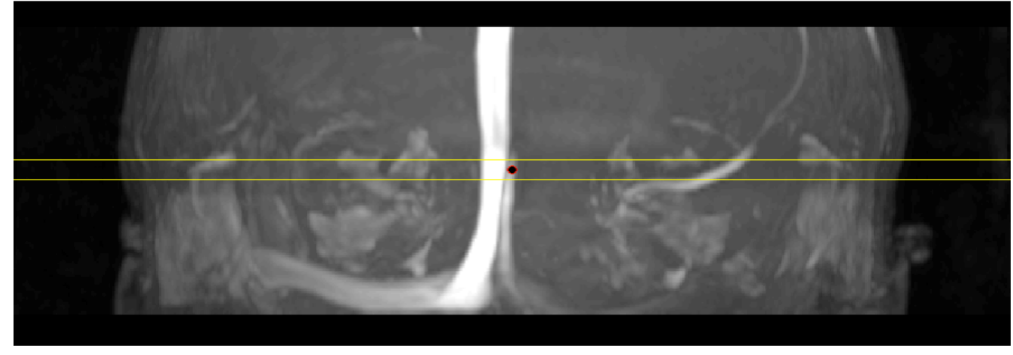
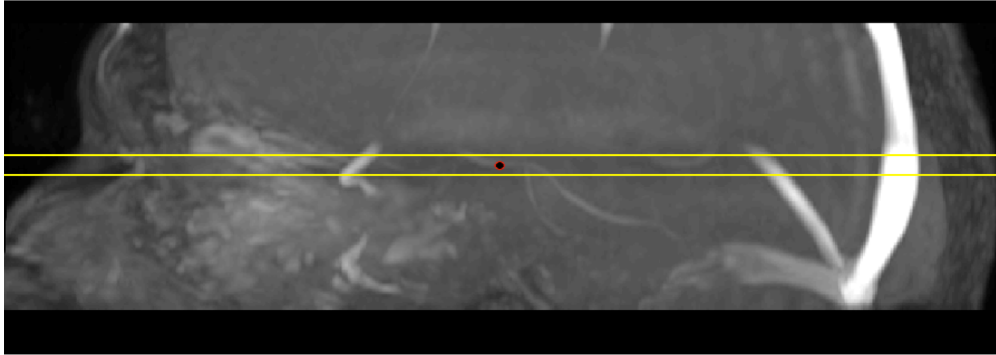
**MRI susceptibility-based
oximetry from
Saggital sinus: venous blood
from brain**



- Velocity through plane (orthogonal the arteries) and Area, thus we get Flow



SUSCEPTIBILITY BASED OXIMETRY



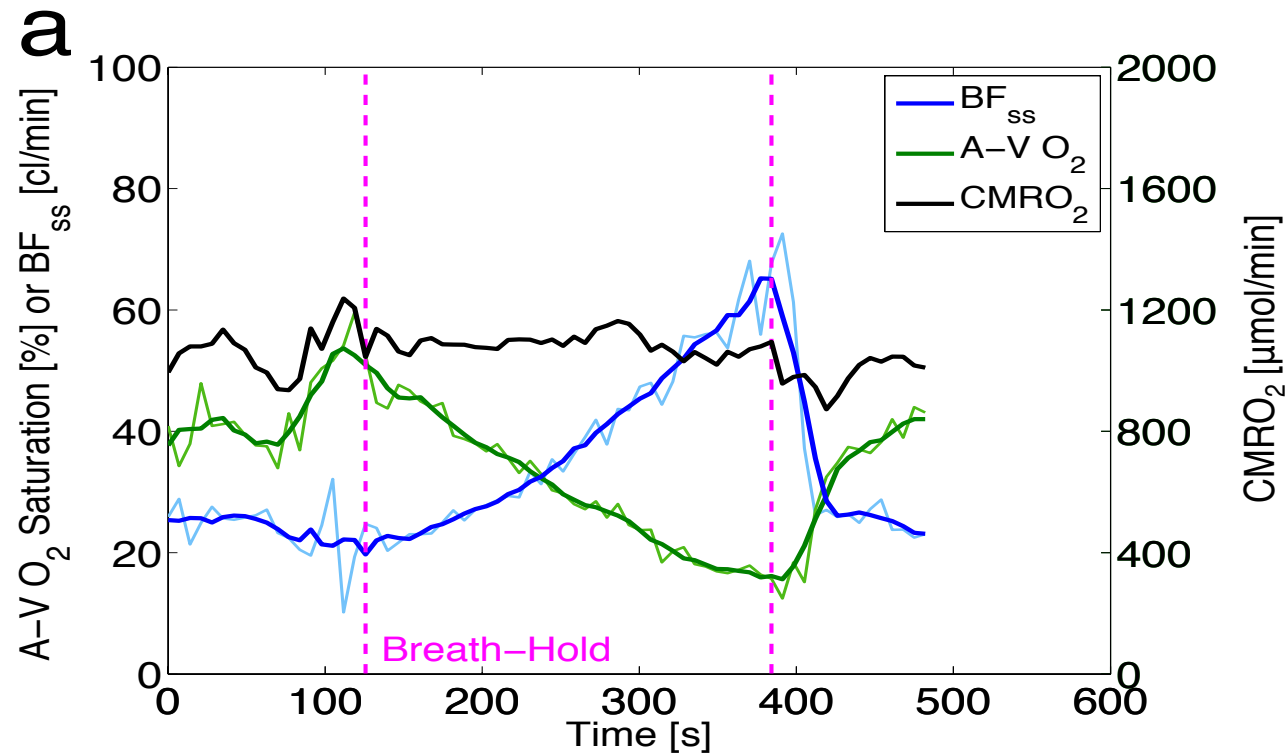
$$SvO_2 = \left(1 - \frac{2 |\Delta\phi_{ss} - \Delta\phi_{tissue}|}{\gamma\Delta TE\Delta\chi_{do} B_0 (\cos^2\theta - 1/3) Hct} \right)$$



Breathhold: $CMRO_2$

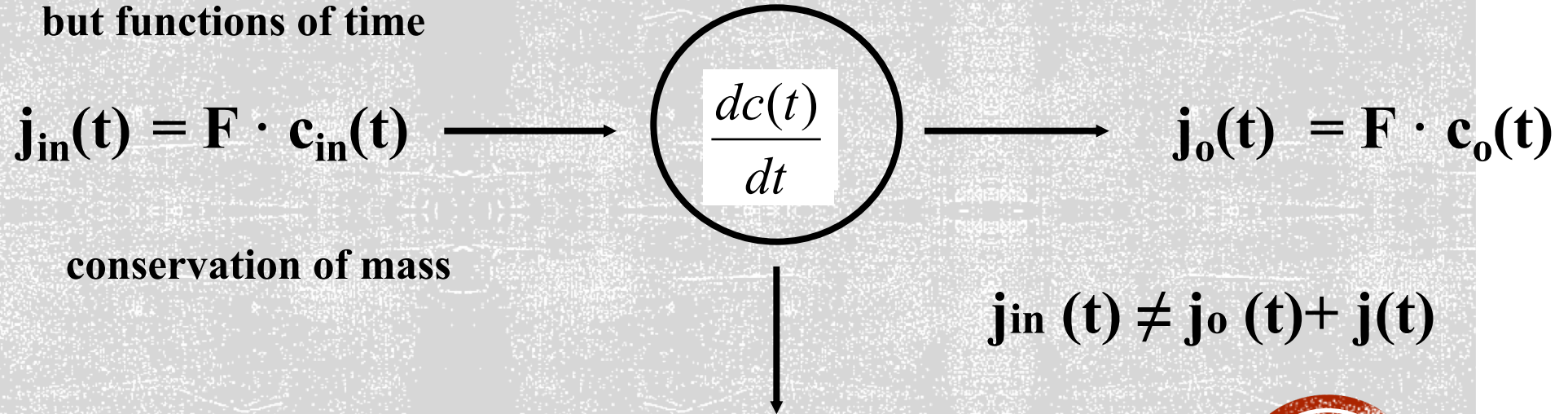
- $CMRO_2 = 4 \cdot [Hgb] \cdot BF_{ss} \cdot (S_a O_2 - S_v O_2)$
- Blood-flow i sagittal sinus (BF_{ss})
- Arteriovenous oxygen-difference ($A-V O_2$)

Vestergaard MB, Larsson HBW. Cerebral metabolism and vascular reactivity during breath-hold and hypoxic challenge in freedivers and healthy controls. J Cereb Blood Flow Metab 2017 .



EXTENDING THE PRINCIPLE OF FICK

The fluxes are not constant, but functions of time The concentration here is not constant

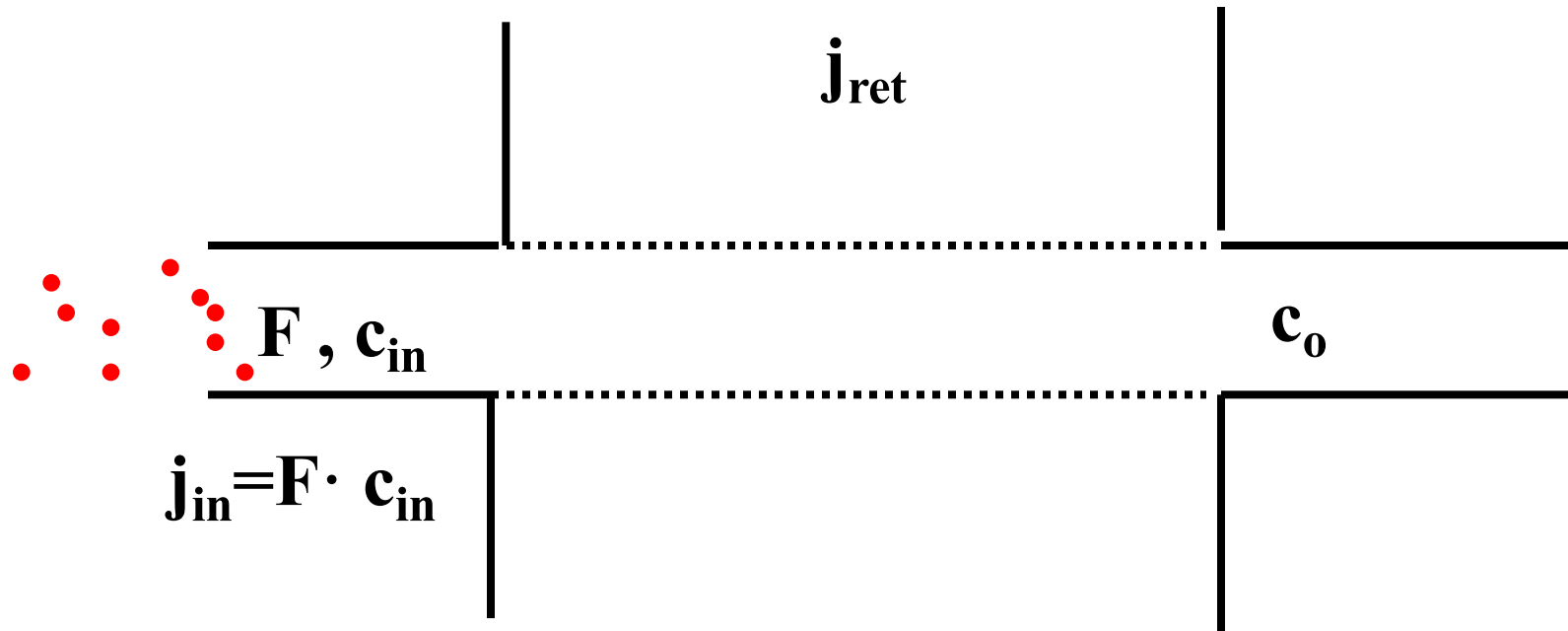


$$v \frac{dc(t)}{dt} = F \cdot c_{in}(t) - F \cdot c_o(t) - j(t) \quad j(t) = K_i \cdot c(t)$$



$$v \frac{dc(t)}{dt} = F \cdot c_{in}(t) - F \cdot c_o(t) - K_i \cdot c(t)$$

EXTRACTION FRACTION

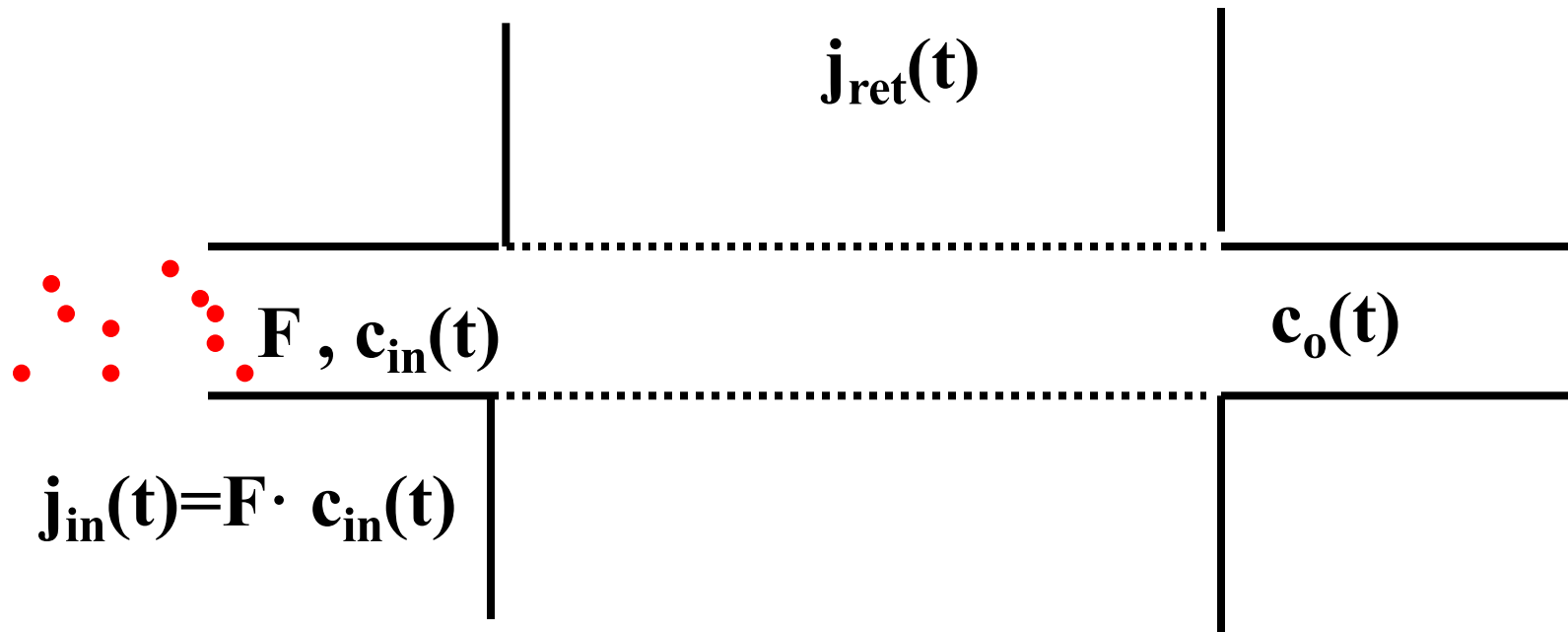


Extraction:
$$E = \frac{j_{ret}}{j_{in}} = \frac{F \cdot c_{in} - F \cdot c_o}{F \cdot c_{in}} = \frac{c_{in} - c_o}{c_{in}}$$

The transmitted fraction = 1-E



EXTRACTION FRACTION

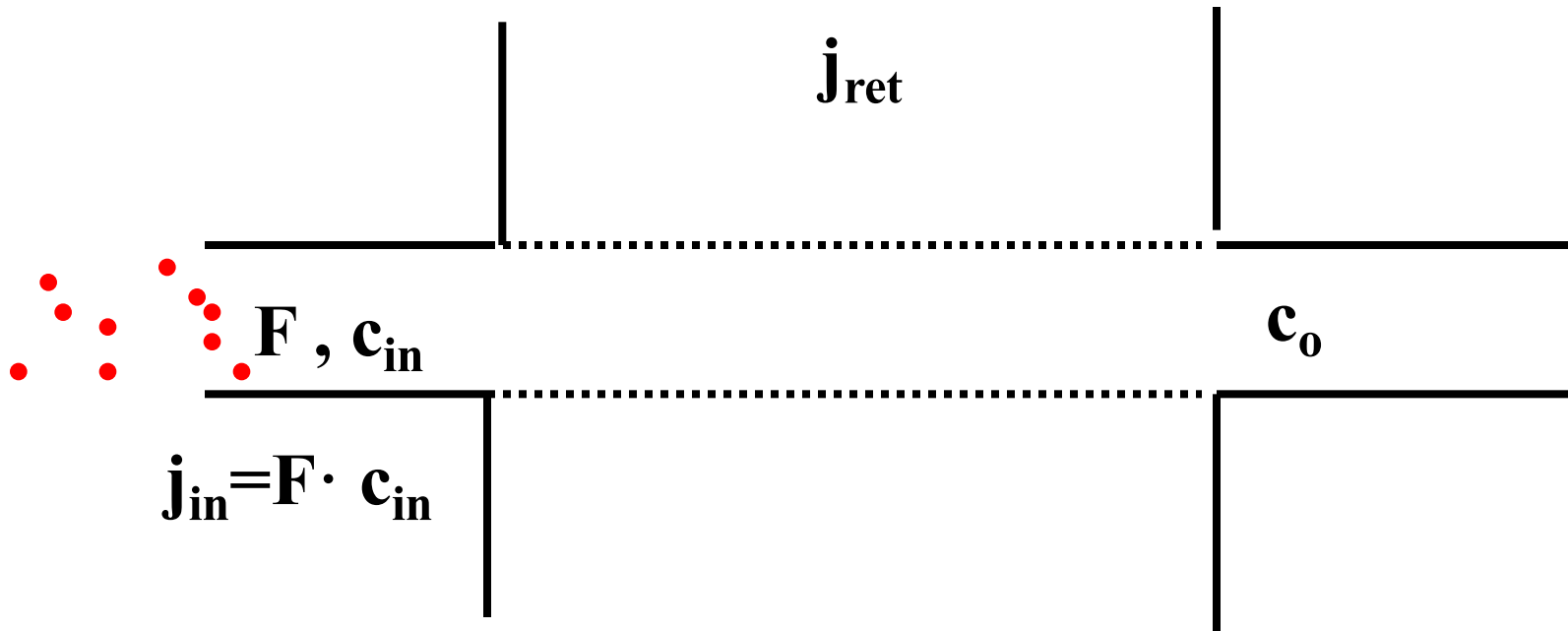


Extraction:
$$E = \frac{j_{ret}(t)}{j_{in}(t)} = \frac{F \cdot c_{in}(t) - F \cdot c_o(t)}{F \cdot c_{in}(t)} = \frac{c_{in}(t) - c_o(t)}{c_{in}(t)}$$

Is E constant?



CLEARANCE



clearance: $Cl = \frac{j_{ret}}{c_{ref}} = \frac{F \cdot c_{in} - F \cdot c_o}{c_{ref}} \quad [Cl] = \text{ml/s}$

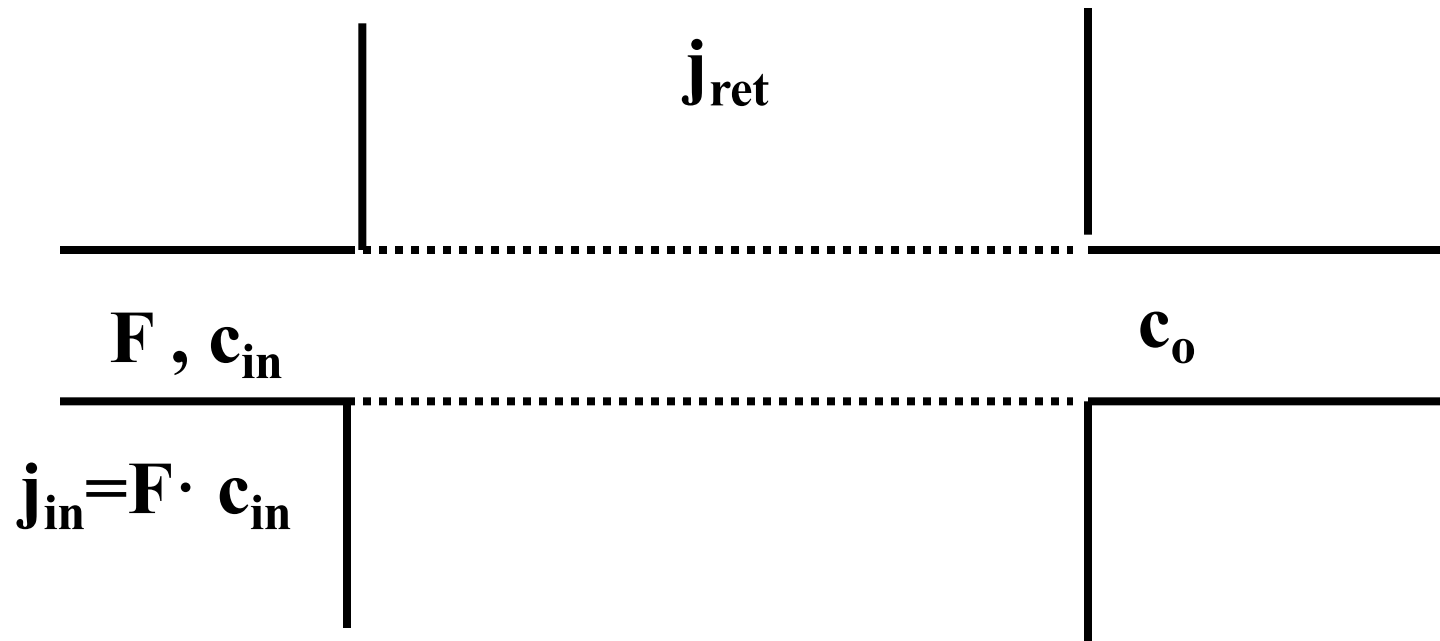


CLEARANCE

It is a fictive flow: the volume of reference fluid containing the indicator amount taken up or cleared per unit time



CLEARANCE



clearance:
$$Cl = \frac{j_{ret}}{c_{ref}} = \frac{j_{ret}}{c_{in}} = \frac{F \cdot c_{in} - F \cdot c_o}{c_{in}} = F \cdot E$$

When $E=1$, Clearance = Flow



BREAK



EXTRACTION, CRONE-RENKIN, PERMEABILITY

Stig P. Cramer, MD, PhD

Post Doc, Functional Imaging Unit

Rigshospitalet, Glostrup



CRONE (1963) & RENKIN (1959) EQUATION

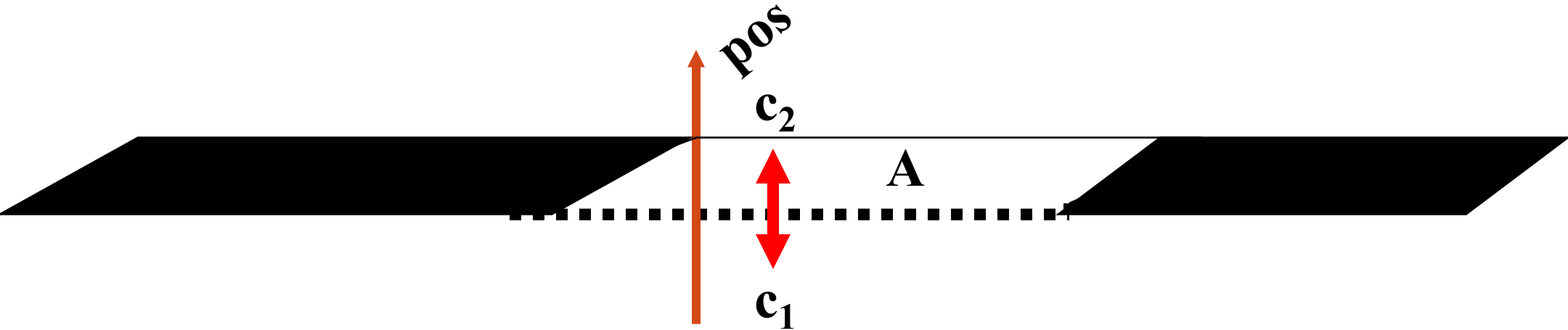
TRANSPORT OVER THE CAPILLARY MEMBRANE



$$c_o = c_{in} \exp(-PS/F)$$



TRANSPORT OVER A MEMBRANE



$j \quad ? \quad c_1 - c_2$

$$J_{1 \rightarrow 2} = PS(c_1 - c_2) \quad PS = \frac{J_{1 \rightarrow 2}}{c_1 - c_2} \quad \frac{\text{mmol}/\text{min}}{\text{mmol}/\text{ml}}$$

$$[PS] = \text{ml}/\text{min}$$



CRONE (1963) & RENKIN (1959) EQUATION

$$c_0 = c_i e^{-\frac{PS}{F}} \Rightarrow \frac{c_0}{c_i} = e^{-\frac{PS}{F}}$$

$$1 - \frac{c_0}{c_i} = 1 - e^{-\frac{PS}{F}} \Rightarrow \frac{c_i - c_0}{c_i} = 1 - e^{-\frac{PS}{F}}$$

$$E = 1 - e^{-\frac{PS}{F}} \wedge Cl = FE \Rightarrow Cl = K_i = F(1 - e^{-\frac{PS}{F}})$$



ACCUMULATION OF TRACER IN TISSUE CAN BE FLOW LIMITED OR DIFFUSION LIMITED

Flow limited : $PS \gg F \rightarrow PS/F$ is large

$$E = 1 - \exp(-PS/F) \quad E \rightarrow 1 \text{ for } PS/F \rightarrow \infty$$

$$Cl = F E \rightarrow F$$



ACCUMULATION OF TRACER IN TISSUE CAN BE FLOW LIMITED OR DIFFUSION LIMITED

Diffusion limited : $PS \ll F \rightarrow PS/F$ small

$$E = 1 - \exp(-PS/F) \quad E \rightarrow 0 \text{ for } PS/F \rightarrow 0$$

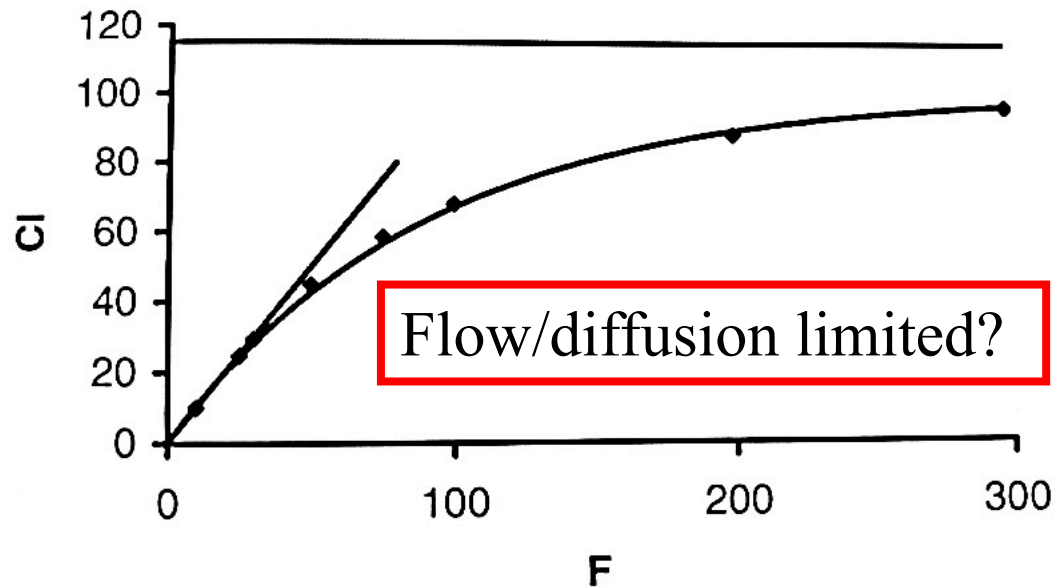
$$E = 1 - \exp(-PS/F) \approx 1 - (1 - PS/F) = PS/F$$

$$CI = F E \rightarrow PS$$



FLOW AND CLEARANCE

Flow og clearance



$E=0.90$ (at rest)

→ Flow limited tracer

Resting $F = 50$ ml/100g/min

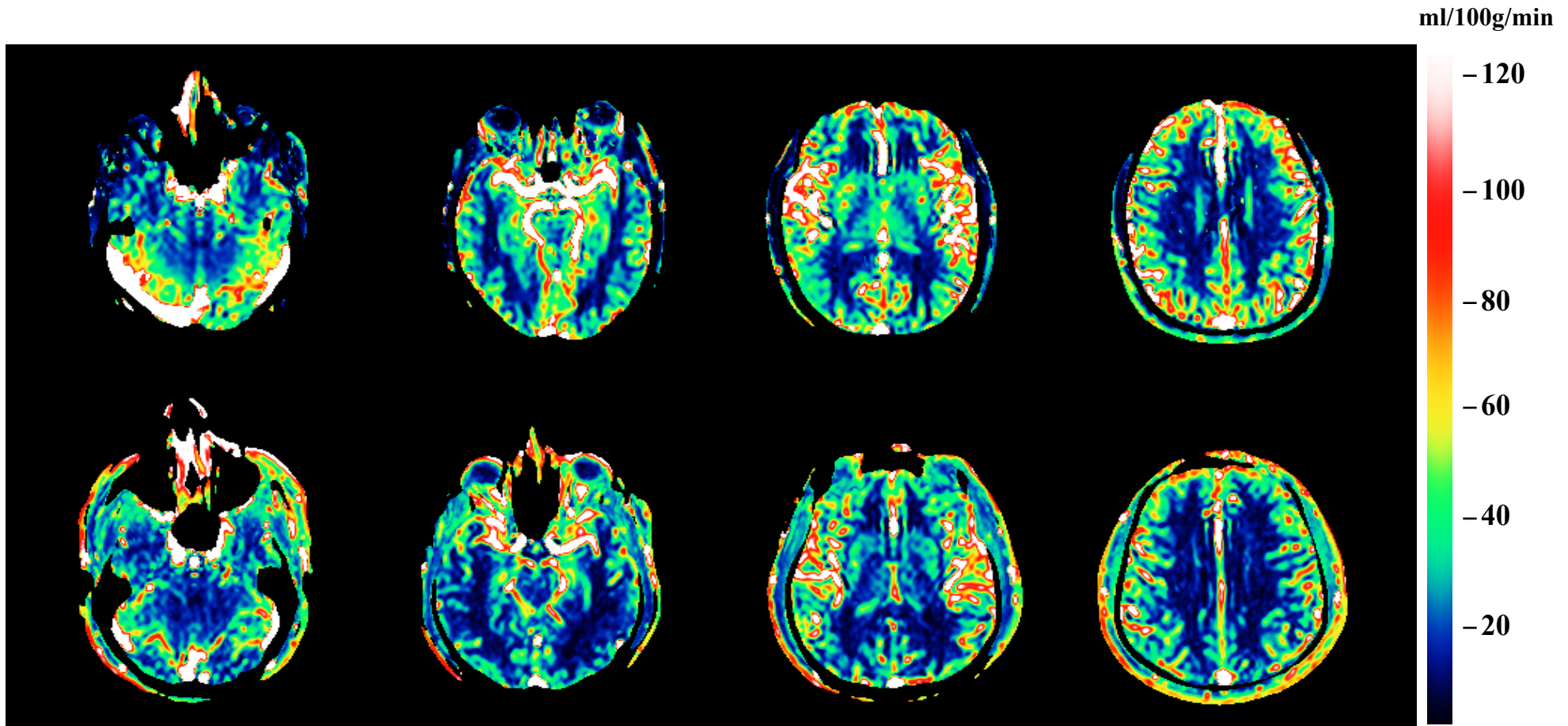
Flow/diffusion limited?

$$E = 1 - e^{\frac{-PS}{F}} \Rightarrow 0.90 = 1 - e^{\frac{-PS}{50}}$$

$$PS = -\ln(0.1) 50 \frac{\text{ml}}{100\text{g min}} = 115 \frac{\text{ml}}{100\text{g min}}$$

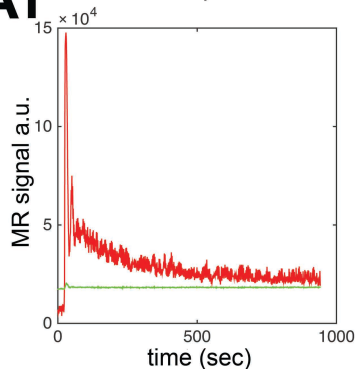


Examples of CBF maps

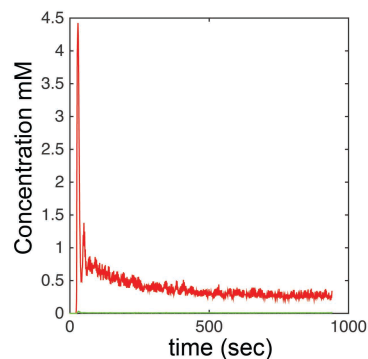
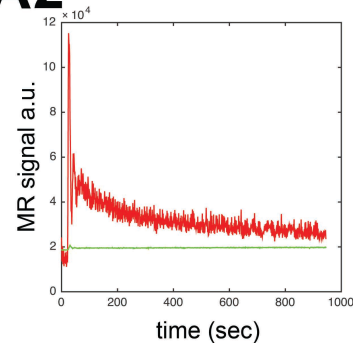


We found perfusion value for ROI's to be **62 ml/100g/min in gray matter** and **21 ml/100g/min in white matter** in 7 patients with acute optic neuritis.

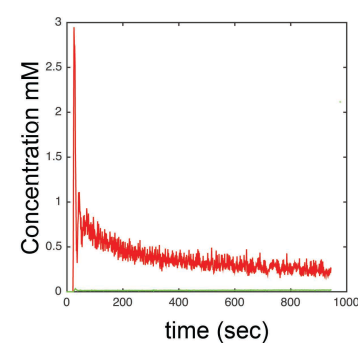
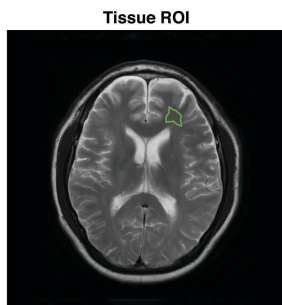


A1 Tissue & Inputfunction

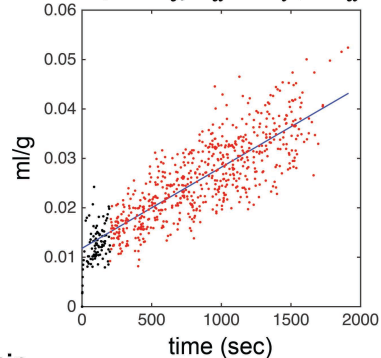
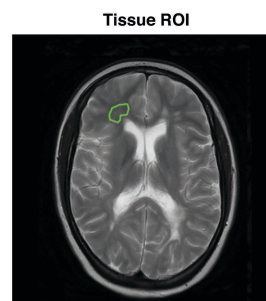
Tissue & Inputfunction

**A2** Tissue & Inputfunction

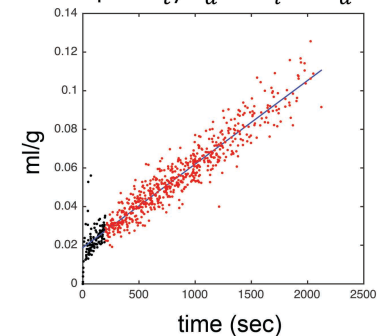
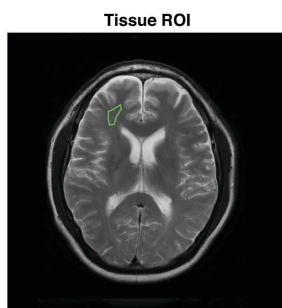
Tissue & Inputfunction

**B1**

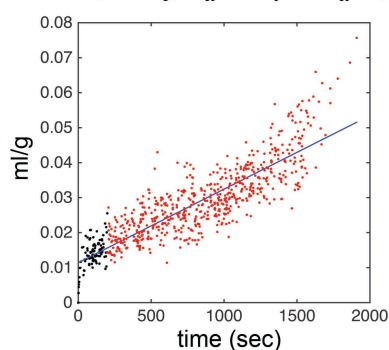
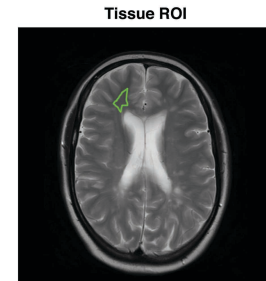
$K_i = 0.0984$ ml/100g/min
 SD of $K_i = 0.0029$ ml/100g/min
 Intercept: $\lambda = 1.18$ ml/100g; SD $\lambda = 0.047$ ml/100g
 pixels-tissue = 142

Patlak plot: $C_t/C_a = K_i \times \Sigma C_a dt / C_a$ **B2**

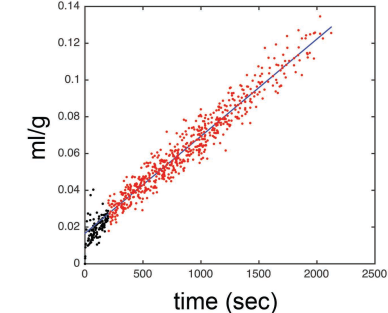
$K_i = 0.260$ ml/100g/min
 SD of $K_i = 0.0036$ ml/100g/min
 Intercept: $\lambda = 1.88$ ml/100g; SD $\lambda = 0.058$ ml/100g
 pixels-tissue = 208

Patlak plot: $C_t/C_a = K_i \times \Sigma C_a dt / C_a$ **C1**

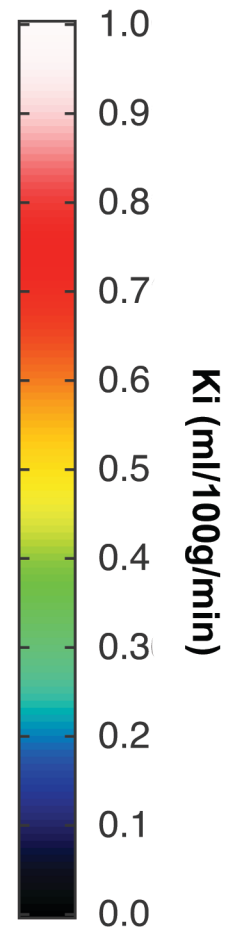
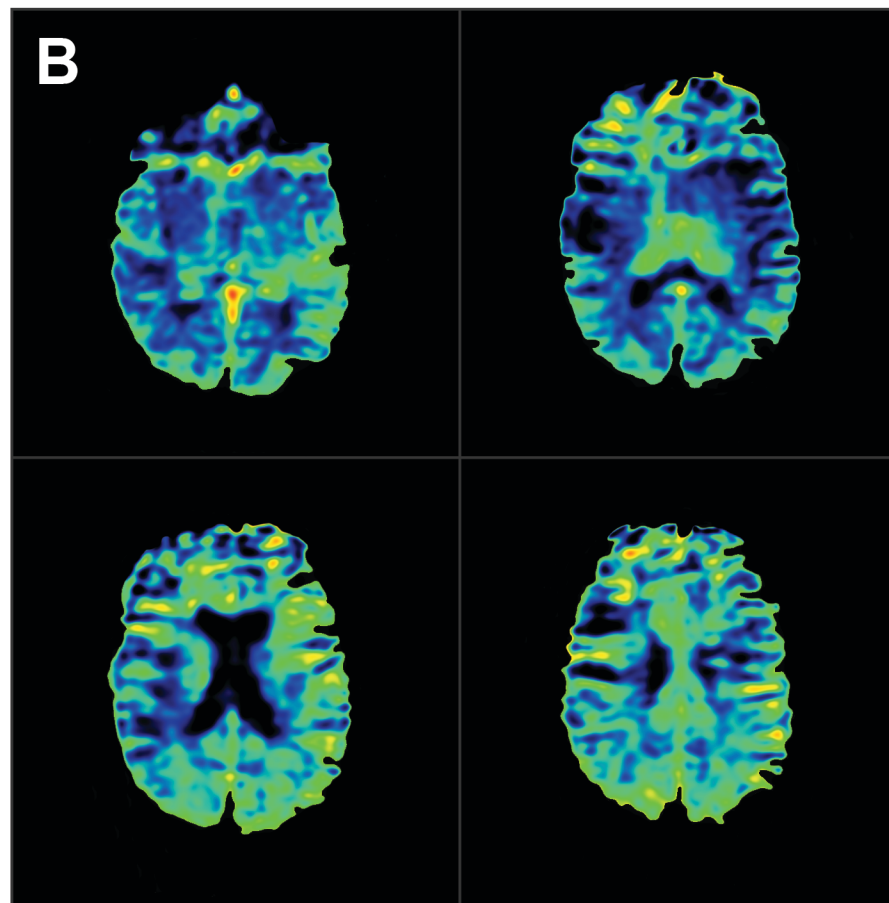
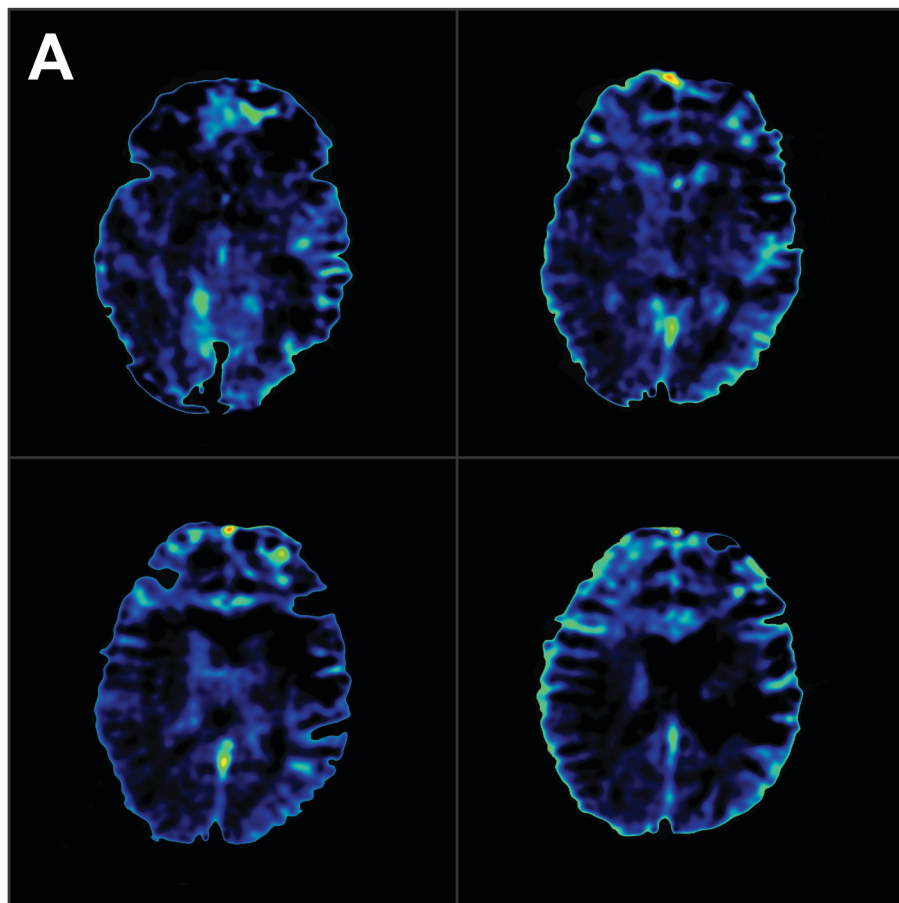
$K_i = 0.126$ ml/100g/min
 SD of $K_i = 0.0034$ ml/100g/min
 Intercept: $\lambda = 1.14$ ml/100g; SD $\lambda = 0.055$ ml/100g
 pixels-tissue = 129

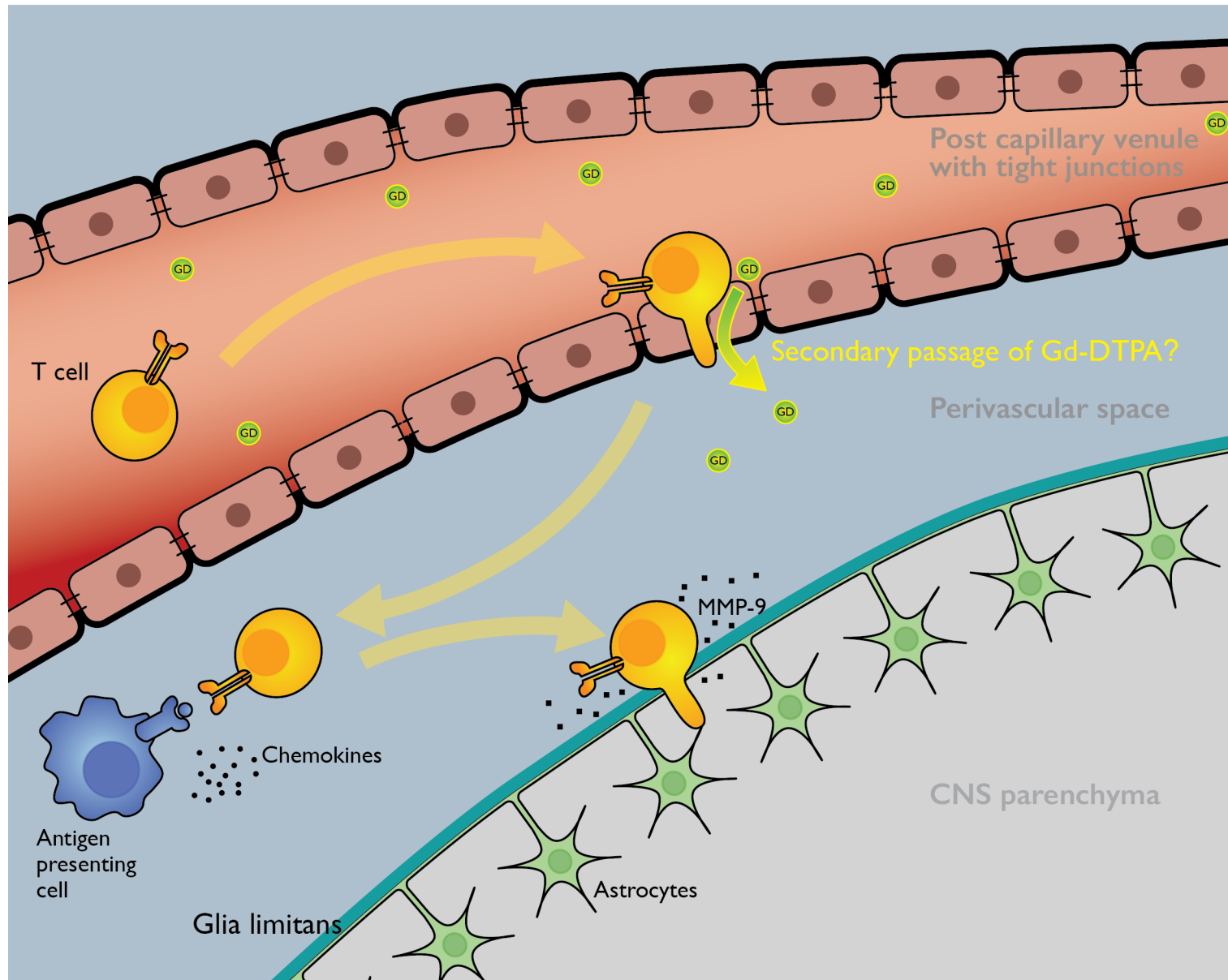
Patlak plot: $C_t/C_a = K_i \times \Sigma C_a dt / C_a$ **C2**

$K_i = 0.317$ ml/100g/min
 SD of $K_i = 0.0032$ ml/100g/min
 Intercept: $\lambda = 1.66$ ml/100g; SD $\lambda = 0.052$ ml/100g
 pixels-tissue = 147

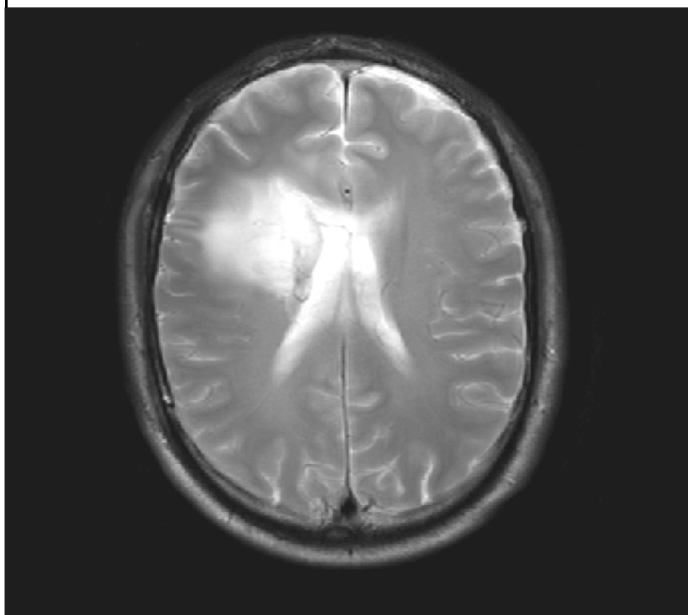
Patlak plot: $C_t/C_a = K_i \times \Sigma C_a dt / C_a$ 

REGIONAL K_i MAPS; ONE WITH AND ONE WITHOUT MULTIPLE SCLEROSIS

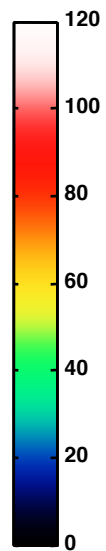
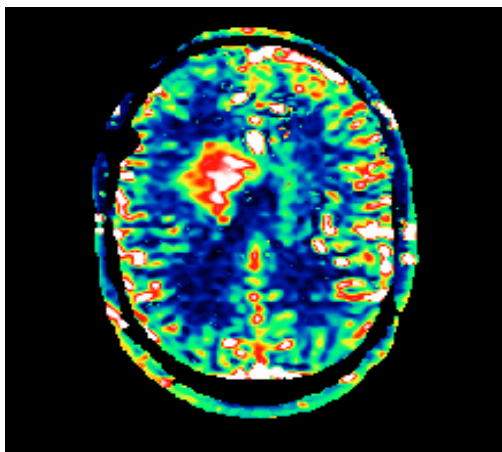




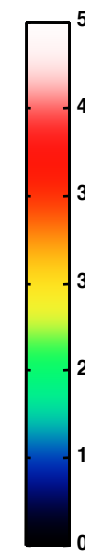
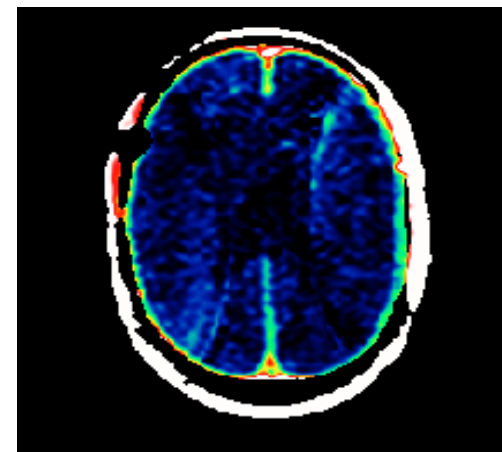
Anatomy, T2w



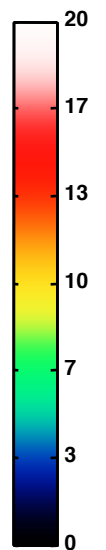
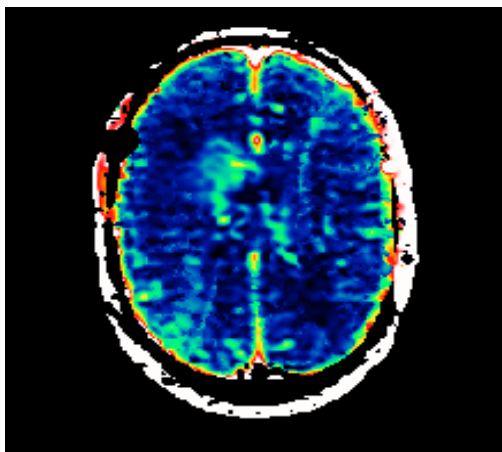
F (ml/100g/min)



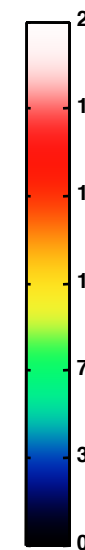
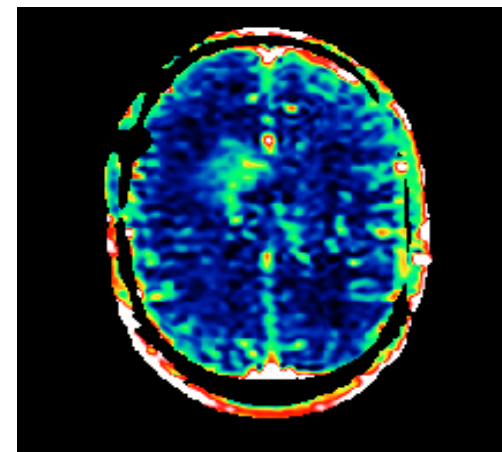
K_i (ml/100g/min)



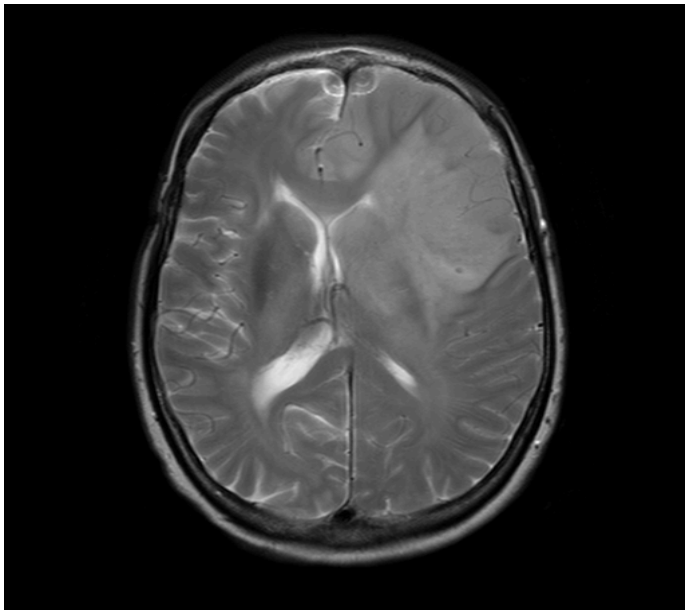
V_d (ml/100g)



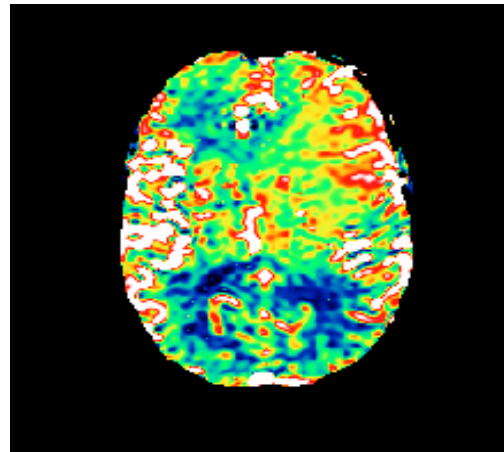
V_b (ml/100g)



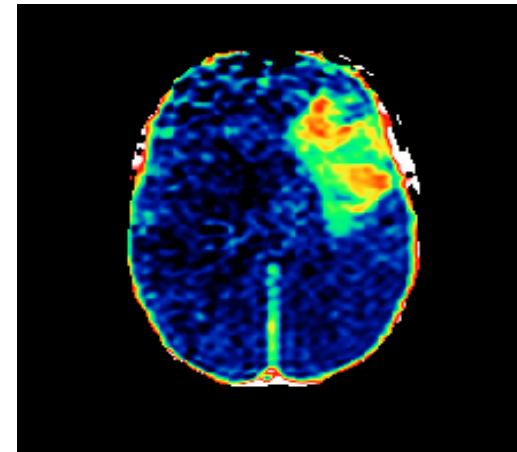
Anatomy, T2w



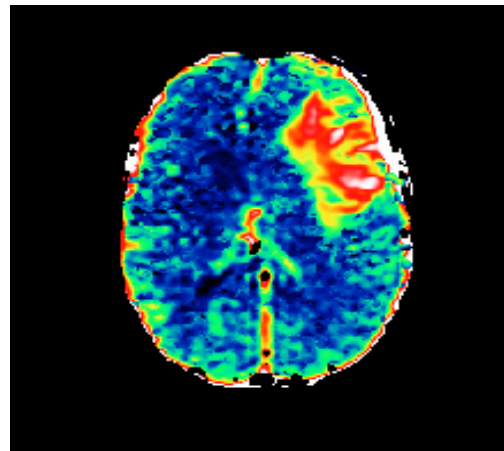
F (ml/100g/min)



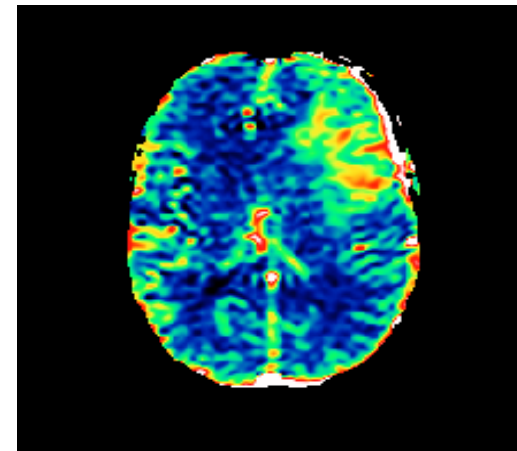
K_i (ml/100g/min)



V_d (ml/100g)



V_b (ml/100g)



BREAK

