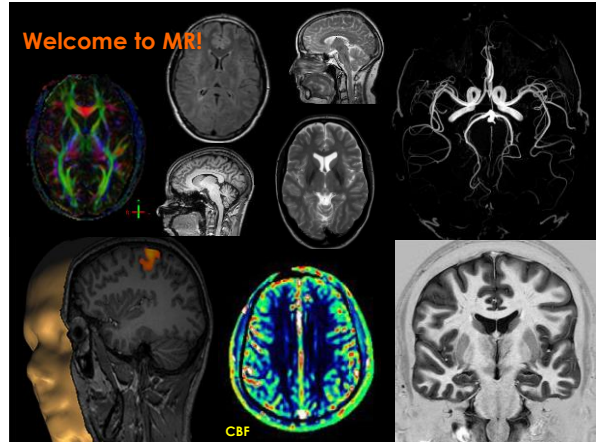


## Introduction to Magnetic Resonance Imaging

Adam Espe Hansen, PET/MR-physicist

Department of Clinical Physiology, Nuclear medicine & PET  
Rigshospitalet

Basic Kinetic Modelling in Molecular Imaging



## Common medical imaging modalities

	CT	PET (with FDG)	MRI (T2 w.)
Images			
Physics	Attenuation of x-rays	Positron emission from radioactive tracer	Magnetic resonance with radio waves



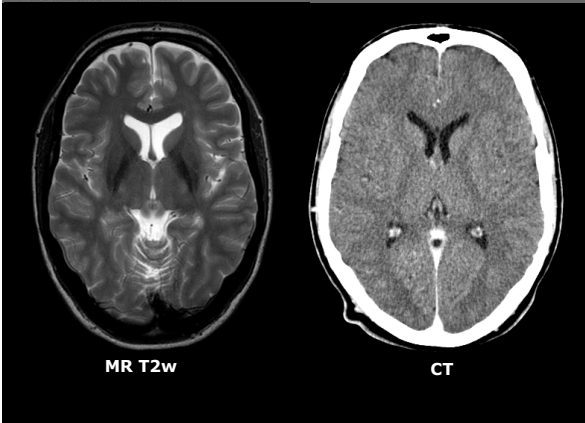
## Introduction to Magnetic Resonance Imaging

### MR Physics:

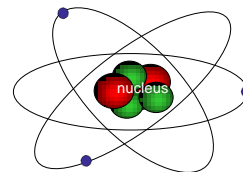
- Nuclear spins
- Magnetization
- Magnetic resonance
- Precession
- Radio waves
- Signal detection
- Spatial encoding
- Relaxation times

### MR Image types:

- T2 weighted
- T1 weighted
- Sequence parameters
- FLAIR
- Diffusion



## Atoms, nuclei, spin

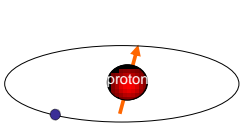


The **spin** of a nucleus depends on the number of neutrons and protons.



**Nuclear spin and magnetism**

Nuclei with spin  $\neq 0$  have magnetic properties.



A proton has spin =  $\frac{1}{2}$ .



**Nuclei with spin**

atom	abundance
$^1\text{H}$	63 %
$^{13}\text{C}$	0.10 %
$^{23}\text{Na}$	0.041 %
$^{31}\text{P}$	0.24 %



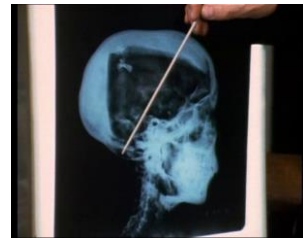
Nuclei with spin  $\neq 0$  in biological tissue.



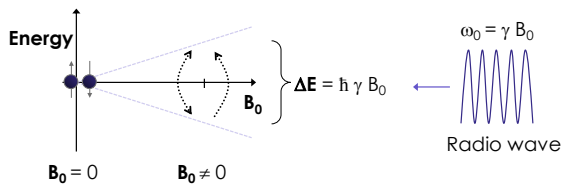
MRI is based on water ...

mongabay.com

**MRI of Tut-ankh-amon?**



**Magnetic resonance, quantum physics**



Nobel prize Rabi (1944) and Bloch/Purcell (1952)



**MR scanner, static magnetic field**

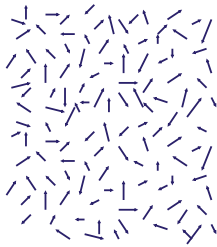


Magnet fields are measured in Tesla (T).  
Commonly used static magnetic fields on clinical scanners: 0.2 T, 0.5 T, 1.0 T, 1.5 T, 3.0 T

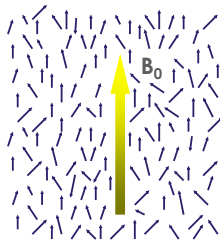
Magnetic field = 3 T



Effect of magnetic field on nuclear spins



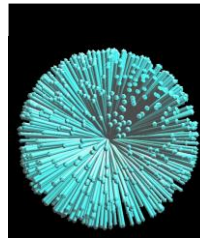
Nuclear spins **outside** field



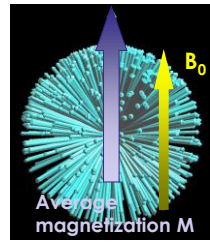
Nuclear spins **in** field



Effect of magnetic field on magnetization



Nuclear spins **outside** field



Nuclear spins **in** field



From Lars G. Hanson, Concepts in Magnetic Resonance Part A, 32A (5), 2008

Magnetization of water in biological tissue

1 voxel contains  
~ 10<sup>23</sup> water molecules

Magnetization in equilibrium

$B_0$ : static magnetic field

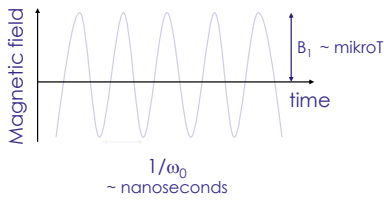
Magnetic resonance

$B_0$ (T)	$\omega_0$ (MHz)
0.2	9
0.5	21
1.0	43
1.5	64
3.0	128

Precession

$B_0$ (T)	$\omega_0$ (MHz)
0.2	9
0.5	21
1.0	43
1.5	64
3.0	128

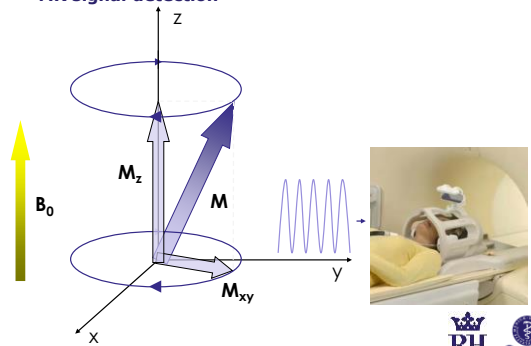
**Radio waves**



RF: a radiowave is a time dependent electric and magnetic field

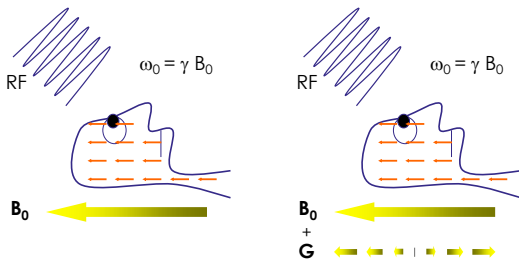


**MR signal detection**

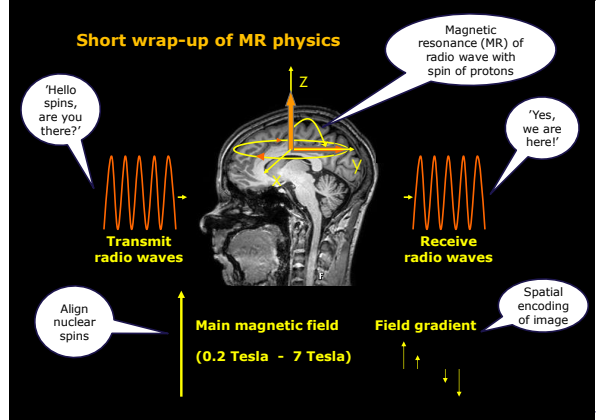


**Slice selection with magnetic field gradient**

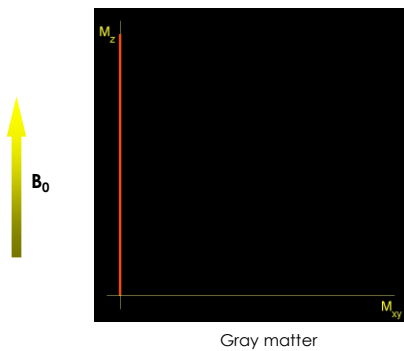
- Spatial encoding of MR images uses magnetic field gradients.
- Gradients can be used for slice selection, frequency- and phase-encoding.



**Short wrap-up of MR physics**



**Relaxation of M**



**Times T1 and T2**

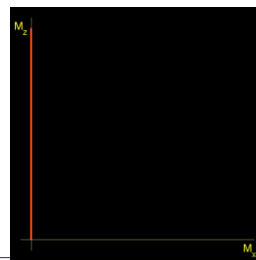
Gray matter:  $T_1 = 950 \text{ ms}$ ,  $T_2 = 100 \text{ ms}$  (1.5 T)

$T_1$ : decay time for  $M_z$

$T_2$ : decay time for  $M_{xy}$

$M_{xy} = M_0 \cdot \exp(-t/T_2)$

$M_z = M_0 \cdot (1 - \exp(-t/T_1))$



### Times T1 and T2

T1 and T2 depend on the microstructure of tissue:

- $T_1 \geq T_2$  for basic physics reasons
- In fluids will T1 and T2 depend on viscosity (T1 is smaller for less viscous fluids).
- T1 and T2 depend on the amount of water in tissue.
- T1 and/or T2 are affected by iron, deoxy-hemoglobin, MR contrast agent, ...
- T1 and T2 are reduced in fat and WM (myelin).
- T1 and T2 depend on the magnetic field (T2 more than T1).

- Gives T1 and T2 image contrast!



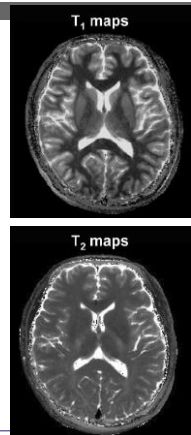
### T1 and T2, measured

	T <sub>1</sub> (ms)	T <sub>2</sub> (ms)
CSF	4500	2200
blood	1200	100-200
GM	950	100
WM	600	80
fat	250	60
muscle	900	50

Haacke et al. (1.5 T)

Synovial fluid	2900	1200
Cartilage	1100	40

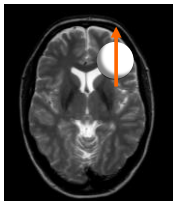
Gold et al. (1.5 T, knee)



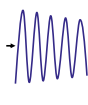
Lu et al. (3 T)



### MR signal loss



T2 weighted image



**Slow signal loss:**  
Mobile nuclei, in particular fluids



**Fast signal loss:**  
Tissue with large immobile molecules, solids

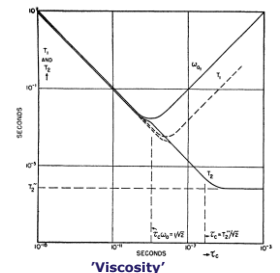
Time scale:  
~ 0.1 – 2 seconds



### Theory of MR in fluids



T<sub>1</sub>, T<sub>2</sub>



PHYSICAL REVIEW VOLUME 74, NUMBER 7 APRIL 1, 1948

Relaxation Effects in Nuclear Magnetic Resonance Absorption\*

N. BLOEMBERGEN,\*\* E. M. FORDYCE, AND R. V. FOLK,\*\*  
Lyons Laboratory of Physics, Cornell University, Ithaca, New York  
(Received December 29, 1947)



### Introduction to Magnetic Resonance Imaging

#### MR Physics:

- Nuclear spins
- Magnetization
- Magnetic resonance
- Precession
- Radio waves
- Signal detection
- Spatial encoding
- Relaxation times

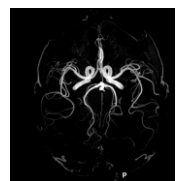
#### MR Image types:

- T2 weighted
- T1 weighted
- Sequence parameters
- FLAIR
- Diffusion

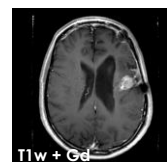


### Sources of MR image contrast

- Water content of tissue
- T1 and T2 of tissue
- Diffusion (Brownian motion of water)
- Flow (blood, CSF)
- Contrast agents (Gd)
- Paramagnetic compounds (...)
- ...



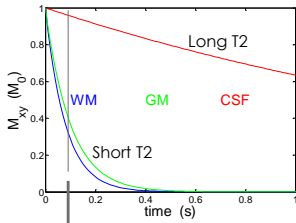
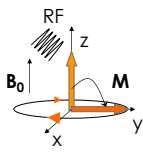
T2w GE



T1w + Gd



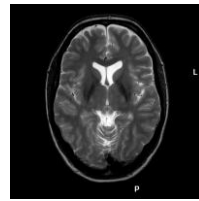
**T2 weighting**



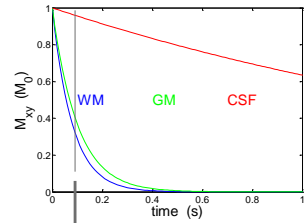
$M_{xy}$  read out after echo time TE (maximization of contrast / noise)



**T2 weighting**



T2 weighted, fat suppr. TR = 3000 ms, TE = 100 ms

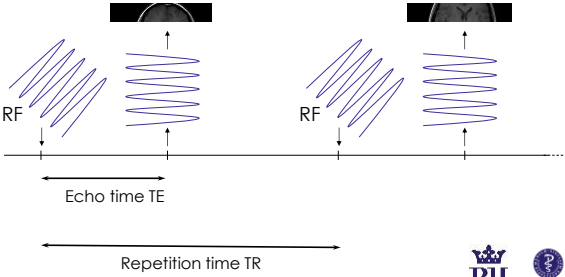


$M_{xy}$  read out after echo time TE

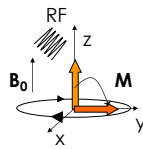
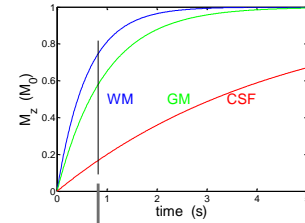
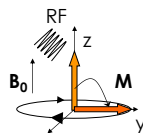


**TR and TE**

In standard MR sequences, one line of the image is read out after a RF excitation



**T1 weighting**

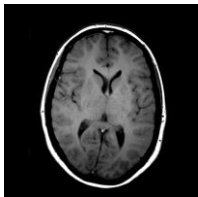


M is flipped again after a repetition time TR

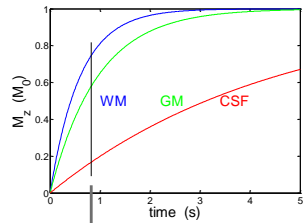
$M_{xy}$  read out after echo time TE



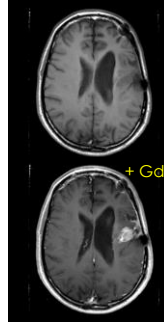
**T1 weighting**



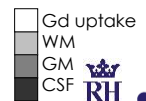
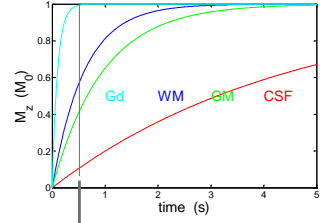
T1 weighted TR = 500 ms, TE = 10 ms



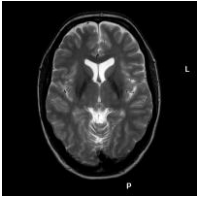
**T1 weighting+ Gd**



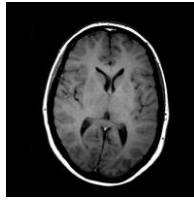
T1 weighted TR = 500 ms, TE = 10 ms



**Sequence parameters**



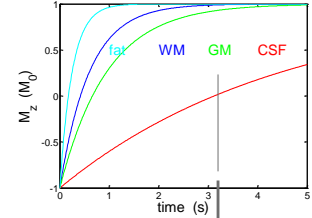
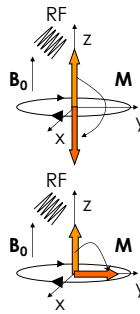
T2 weighted, fat suppr.  
TR = 3000 ms, TE = 100 ms



T1 weighted  
TR = 500 ms, TE = 10 ms

	TR	short	long
TE		short	long
short		T1 w	proton density
long		-	T2 w

**IR - FLAIR**

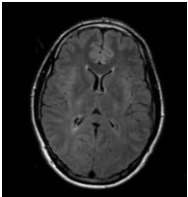


M is flipped again after a inversion time TI

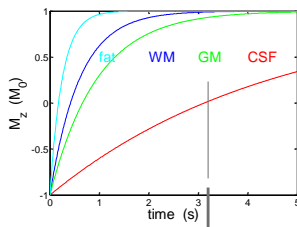
CSF is 'nulled'



**IR - FLAIR**



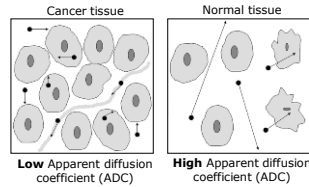
FLAIR, T2 weighted  
TR = 11000 ms, TE = 125 ms,  
TI = 2800 ms



GM  
WM  
CSF



**MR Diffusion Weighted Imaging**

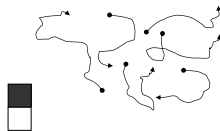


Koh, Collins, AJR (2007)

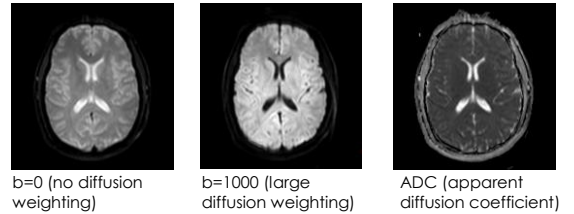


**Diffusion weighted imaging**

- T2 weighted sequence with additional diffusion weighting
- Diffusion weighting: sensitization to the Brownian motion of water molecules
- Large diffusion: less signal  
Small diffusion: more signal



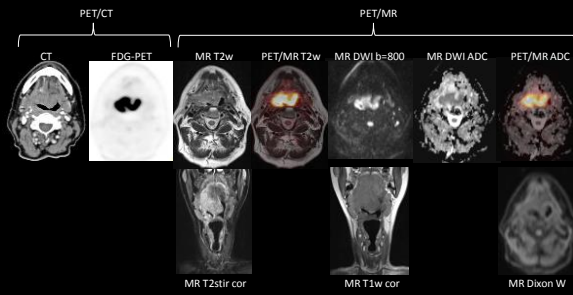
**Diffusion weighted imaging**



$$ADC = -1/b \cdot \ln(\text{Image}_b / \text{Image}_0)$$



### PET/MR with DWI versus PET/CT in head/neck



/J. Löfgren, data from study by J. Rasmussen, B.M. Fischer et al.

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